

Inverse Problems and MRAI

Mapping the pulse wave velocity

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Doctoral Program
Computational Mathematics

Numerical Analysis and Symbolic Computation



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Introduction

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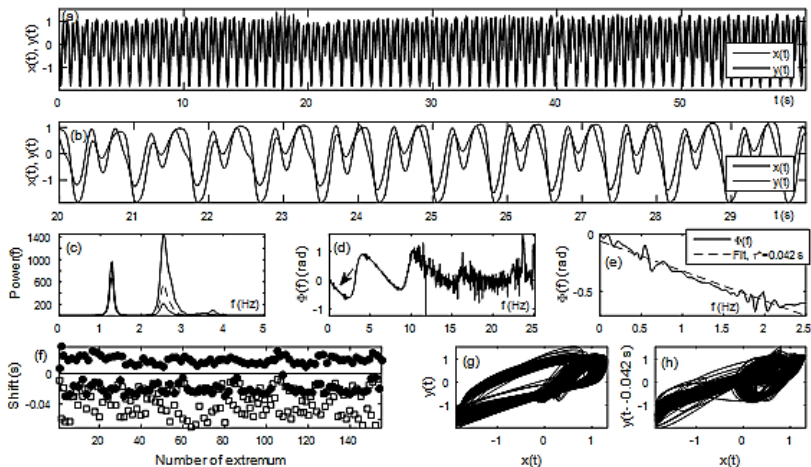
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Estimate the PWV from fMRI data!

Three natural questions:

- What is the PWV?
- Why do we want to estimate it?
- How can we estimate it?

Pulse Wave Velocity



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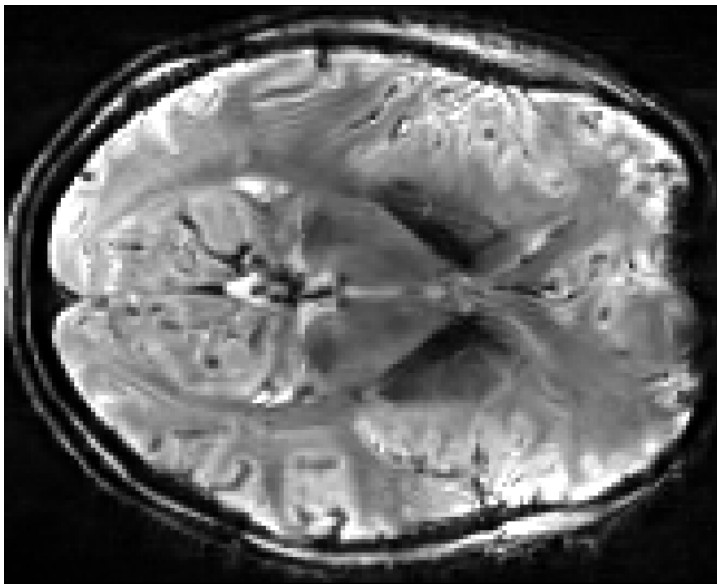
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The parameters are

- h - vessel wall thickness,
- E - vessel wall's Young modulus,
- d - vascular diameter,
- ρ_B - density of the blood.



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MRAI = Magnetic Resonance **Advection** Imaging

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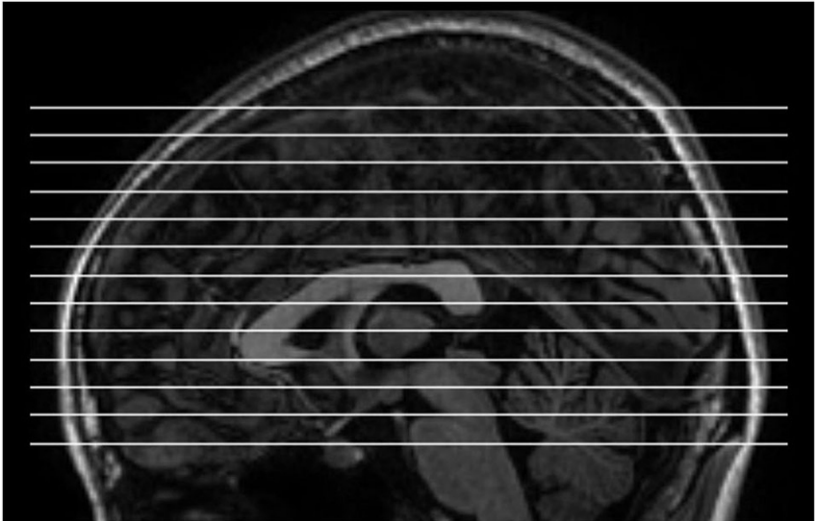
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- Treatment of boundary conditions.
- Partial data \longleftrightarrow slice-time-acquisition problem.

Slice-Time Acquisition



Solution Strategy - Discretization

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The fMRI data ρ is only available at points

$$(x_i, y_j, z_k, t_{k,l})$$

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where

$$x_i = x_0 + i\Delta x, \quad y_j = y_0 + j\Delta y, \quad z_k = z_0 + k\Delta z, \\ t_{k,l} = (k + (K + 1)l)\Delta t,$$

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Idea: Discretize the advection equation according to the data!!

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The continuous advection equation

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then becomes a discrete linear system of equations:

$$\begin{aligned} \frac{\rho_{i,j,k,l} - \rho_{i,j,k,l-1}}{(K+1)\Delta t} + D_{x_i} \rho_{i,j,k,l} v_{1,i,j,k} \\ + D_{y_j} \rho_{i,j,k,l} v_{2,i,j,k} + D_{z_k} \rho_{i,j,k,l} v_{3,i,j,k} = 0, \end{aligned}$$

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where

$$\rho_{i,j,k,l} = \rho(x_i, y_j, z_k, t_{k,l}), \quad v_{m,i,j,k} = v_m(x_i, y_j, z_k), \quad m = 1, 2, 3.$$

Discretization - Finite Differences

$$D_{x_i} \rho_{i,j,k,l} := \begin{cases} \frac{\rho_{i+1,j,k,l} - \rho_{i-1,j,k,l}}{2\Delta x}, & 1 \leq i \leq I-1 \\ \frac{\rho_{1,j,k,l} - \rho_{0,j,k,l}}{\Delta x}, & i = 0 \\ \frac{\rho_{I,j,k,l} - \rho_{I-1,j,k,l}}{\Delta x}, & i = I \end{cases}$$

$$D_{y_j} \rho_{i,j,k,l} := \begin{cases} \frac{\rho_{i,j+1,k,l} - \rho_{i,j-1,k,l}}{2\Delta y}, & 1 \leq j \leq J-1 \\ \frac{\rho_{i,1,k,l} - \rho_{i,0,k,l}}{\Delta y}, & j = 0 \\ \frac{\rho_{i,J,k,l} - \rho_{i,J-1,k,l}}{\Delta y}, & j = J \end{cases}$$

Discretization - Finite Differences

$$D_{z_k} \rho_{i,j,k,l} := \begin{cases} \frac{(1-r)(\rho_{i,j,k+1,l} - \rho_{i,j,k-1,l+1}) + r(\rho_{i,j,k+1,l-1} - \rho_{i,j,k-1,l})}{2\Delta z}, & 1 \leq k \leq K-1, 1 \leq l < L \\ \frac{(1-r)\rho_{i,j,k+1,L} - (1+r)\rho_{i,j,k-1,L} + r(\rho_{i,j,k+1,L-1} + \rho_{i,j,k-1,L-1})}{2\Delta z}, & 1 \leq k \leq K-1, l = L \\ \frac{(1-r)\rho_{i,j,1,l} + r\rho_{i,j,1,l-1} - \rho_{i,j,0,l}}{\Delta z}, & k = 0, 1 \leq l \leq L \\ \frac{\rho_{i,j,K,l} - (1-r)\rho_{i,j,K-1,l+1} - r\rho_{i,j,K-1,l}}{\Delta z}, & k = K, 1 \leq l < L \\ \frac{\rho_{i,j,K,L} - (1+r)\rho_{i,j,K-1,L} + r\rho_{i,j,K-1,L-1}}{\Delta z}, & k = K, l = L \end{cases}$$

$$r := \frac{1}{K+1}$$

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We denote the solution $\vec{\rho}$ of this equation with $\rho(\vec{v}, \vec{\rho}_0)$.

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$$\langle (\vec{v}, \vec{\rho}_0), (\vec{x}, \vec{w}_0) \rangle_{\mathcal{X}} := \vec{v}^T H \vec{x} + \vec{\rho}_0^T \vec{w}_0,$$

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We can now write our problem in standard form, i.e.,

$$" F (\vec{v}, \vec{\rho}_0) = (\vec{\rho}^\delta, \vec{\rho}_0^\delta) "$$

Derivative and Adjoint

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The Frechet derivative is given by

$$F'(\vec{v}, \vec{\rho}_0)(\Delta\vec{v}, \Delta\vec{\rho}_0) = (\rho'(\vec{v}, \vec{\rho}_0)(\Delta\vec{v}, \Delta\vec{\rho}_0), \Delta\vec{\rho}_0),$$

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It's adjoint is given by

$$F'(\vec{v}, \vec{\rho}_0)^*(\vec{w}, \vec{w}_0) = \begin{pmatrix} H^{-1} \left(-D_A(\vec{v}, \rho(\vec{v}, \vec{\rho}_0))^T + b'_{\Delta\vec{\rho}_0}(\vec{v}, \vec{\rho}_0)^T \right) A(\vec{v})^{-T} \vec{w} \\ b'_{\Delta\vec{v}}(\vec{v}, \vec{\rho}_0)^T A(\vec{v})^{-T} \vec{w} + \vec{w}_0 \end{pmatrix}.$$

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$$\implies F(\vec{v}, \vec{\rho}_0) := (\rho(\vec{v}, \vec{\rho}_0), \vec{\rho}_0, D\vec{v}).$$

Choosing the matrix H

Remember the inner product:

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- **Solution 2:** Use Wavelets instead of H .

Computation Method

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Landweber type gradient method:

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Discrepancy principle:

$$\|y^{\delta} - F(x_{k_*}^{\delta})\| \leq \tau \delta \leq \|y^{\delta} - F(x_k^{\delta})\|, \quad 0 \leq k \leq k_*.$$

Sparsity

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Shrinkage function:

$$S_{\tau,p}(x) = \begin{cases} \operatorname{sgn}(x) \max(|x| - \tau, 0), & p = 1, \\ G_{\tau,p}^{-1}(x), & p \in (1, 2], \end{cases}$$

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Resulting iteration:

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⇒ *Runs on a standard home computer in acceptable time!!!*

(Real-world data set has 3 million unknowns)

Simulation Outline

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- 1 Prepare a phantom of size $40 \times 30 \times 30$ featuring several vessels of different thickness and orientation.

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Steps of the data creation:

- ① Prepare a phantom of size $40 \times 30 \times 30$ featuring several vessels of different thickness and orientation.
- ② For every vessel:
 - Choose a constant velocity \bar{v} pointing in vessel direction.

Simulation Outline

Steps of the data creation:

- ① Prepare a phantom of size $40 \times 30 \times 30$ featuring several vessels of different thickness and orientation.
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 - Choose a constant velocity \bar{v} pointing in vessel direction.
 - Choose an initial signal ρ_0 of sinusoidal form.

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 - Sample at the right space-time points to get $\rho_{i,j,k,l}$
- ❸ Combine the vessel contributions.
- ❹ Add a random data error of magnitude δ .

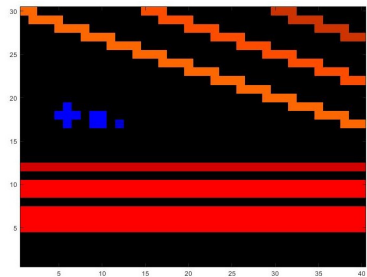
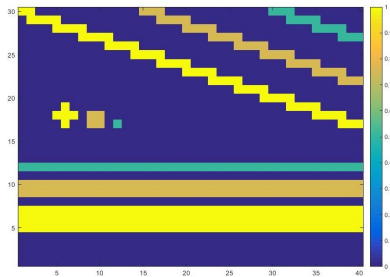
Simulation Outline

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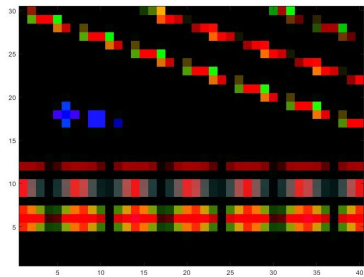
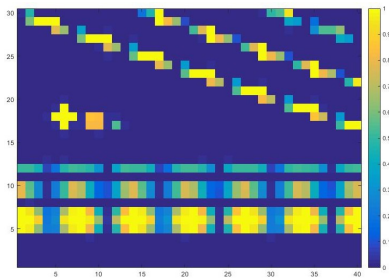
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⇒ Run the algorithm using the discrepancy principle ($\tau = 1.1$).

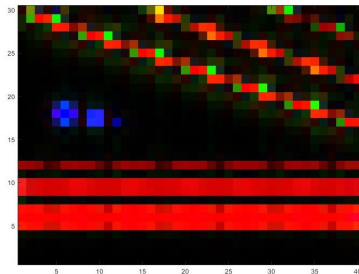
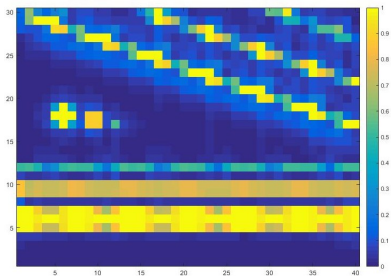
Simulation Phantom - MIP and direction MIP



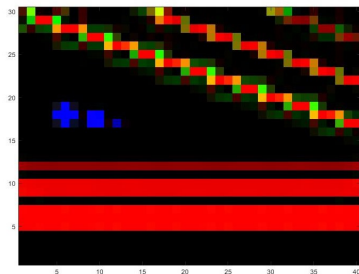
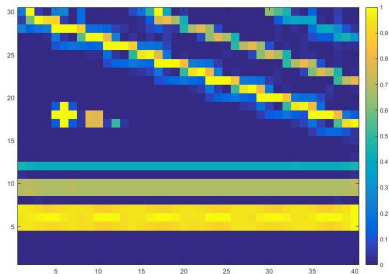
Results - Pure Method



Results - Divergence-Free



Results - Divergence-Free + Sparsity



Natural Stimulation Data Set

Natural Stimulation Data Set

Specifications:

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- Publicly available natural stimulation dynamic EPI data.

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- Data has dimension $132 \times 175 \times 48$.
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- Pulse repetition time (TR) of 2 seconds.
- Eight 15 minutes long segments for each subject.

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Algorithm specifics:

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Algorithm specifics:

- First 20 seconds of second segment were used.

Natural Stimulation Data Set

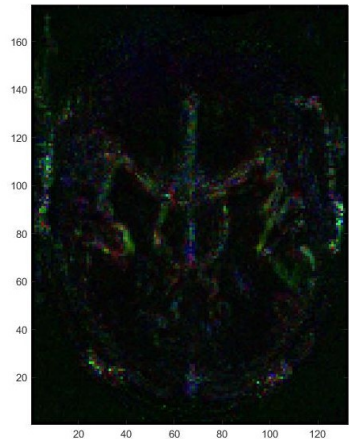
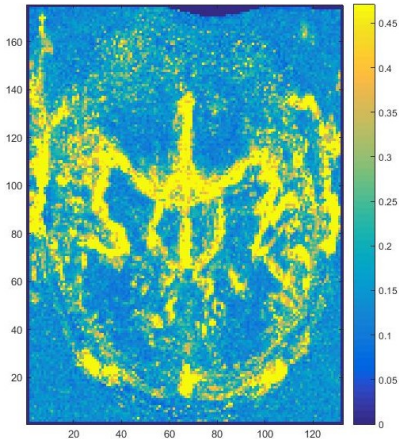
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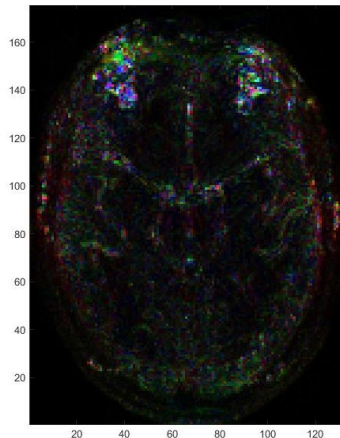
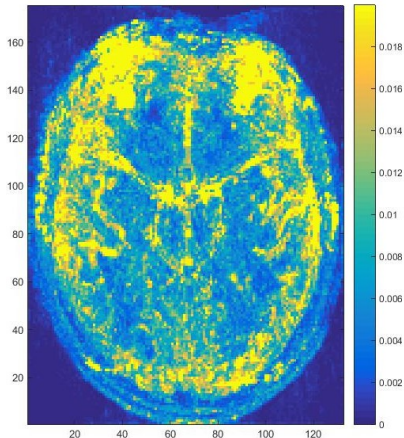
Algorithm specifics:

- First 20 seconds of second segment were used.
- **Stopping rule:** Residual decrease check.

Regression Approach - Results



New Approach - Results



End

Thank you for your attention!